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## Thermodynamic Stability of Myoglobin-Poly(Ethylene Glycol) Bioconjugates: a Calorimetric Study

Chiara Pelosi <sup>a, b, \*</sup>, Francesca Saitta <sup>c, \*</sup>, Frederik R. Wurm <sup>b</sup>, Dimitrios Fessas <sup>c</sup>, Maria Rosaria Tinè <sup>a</sup> and Celia Duce <sup>a</sup>.

<sup>a</sup>: Dipartimento di Chimica e Chimica Industriale, Università di Pisa, Via Moruzzi, 56124, Pisa, Italy.

<sup>b</sup>: Max-Planck-Institut für Polymerforschung, Ackermannweg 10, 55128 Mainz, Germany.
<sup>c</sup>: Dipartimento di Scienze per gli Alimenti, la Nutrizione e l'Ambiente, DeFENS, Università degli Studi di Milano, Via Celoria 2, 20133, Milano, Italy

\* These authors contributed equally to the work.

Corresponding authors: Maria Rosaria Tinè, <u>mariarosaria.tine@unipi.it</u>, +39 0502219268; Dimitrios Fessas, <u>dimitrios.fessas@unimi.it</u>, +39 0250319219.

Graphical Abstract



The image of myoglobin's structure in this picture was taken from the RCSB PDB (www.rcsb.org) of PDB ID 1MBN (Watson, H. C. (1969) The stereochemistry of protein myoglobin Prog. Staroocham. 4: 299].

### Highlights

- The myoglobin denaturation mechanism remains unaffected upon PEGylation
- PEGylation causes a thermal destabilization of myoglobin but enhances reversibility
- PEGylation decreases the solvent-exposed surface of the myoglobin denatured state

#### Abstract

PEGylated proteins are widely used for therapeutic applications, therefore a fundamental understanding of the conjugates' structure and their behaviour in solution is essential to promote new developments in this field. In the present work, myoglobin-poly(ethylene glycol) conjugates were synthesized and studied by differential scanning calorimetry and UV-visible spectroscopy to obtain information on the bioconjugates' thermodynamic stability, also focusing on PEG's role on the solvent-protein surface interaction. The overall results of this study indicated a thermal destabilization of the protein that follows the extent of the bioconjugation without, however, compromising the native structure which remains functional. Moreover, the myoglobin PEGylation prevented the post-denaturation aggregation phenomena and enhanced the protein thermal reversibility. The thermodynamic interpretation of the data indicated that the bioconjugation influences the solvent-exposed protein surface difference between native and denatured state, contributing to the interpretation of the overall protein modification and functionality.

### Keywords: PEGylation, calorimetry, protein unfolding, unfolding reversibility, proteinpolymer conjugation.

#### 1. Introduction

The biotechnology evolution of the last century has underlined the great potentialities of proteins and peptides as therapeutic agents. Nowadays more than 90 protein based compounds are industrially produced and used as potent drugs for the treatment of severe diseases [1,2]. Despite their usefulness, they often exhibit several drawbacks, among which there are short shelf-life, low solubility in water and short life time inside the body [3]. Several strategies have been developed to avoid or decrease these limits, reducing the production costs of the drugs and their dosing frequency for patients [4]. One of the most promising strategies is bioconjugation, that consists in the covalent attachment of synthetic polymers to the proteins in order to form protein-polymer conjugates [5].

Poly(ethylene glycol) (PEG) is the most common polymer in bioconjugation [6]. Today there are 13 PEG-protein conjugates approved from U.S. Food and Drug Administration and used for therapeutic purposes, while many others are currently under clinical trials [7–10]. The conjugates can perform several functions: replacement therapies for native enzyme deficiencies (Adagen®, Oncaspar®, Krystexxa®), stimulation of immune responses (PEG-Intron®, PEGASYS®, Plegridy®), regulation of blood cells production (Mircera®, Omontys®, Adinovate®), stimulation or inhibition in the production of important regulation substances (Neulasta®, Somavert®, Macugen®) and can be used against several diseases. The covalent bond of the polymer induces the formation of a protective shield around the protein-based drug, often resulting in an improvement of some properties, major drug solubility, less *in vivo* and *in vitro* aggregation, less immunogenicity and allergenicity, minor degradation and opsonisation and minor kidney clearance [11–14]. The overall effect is an improvement in the drug pharmacokinetics, with an increasing life time and a reduction of the necessary dosage frequency for patients. Moreover the PEGylation of surfaces reduces the adsorption

of other proteins that occurs in a physiological media, thanks to the high hydration of the hydrophilic polyether backbone and to an increased steric repulsion on the surface [15]. These shielding features are indicated as stealth effect of PEG.

Beyond the pharmacologic evaluation, the thermodynamic and structural protein stability and its residual activity after the bioconjugation process [16–19] provide important information in order to understand properties and potentialities of new pharmaceutical proteins.

However, few studies regarding the thermodynamic stability of protein-polymer conjugates appear in the literature [20–23] and despite some hypotheses being advanced [23,24], the molecular mechanism by which PEGylation changes the protein thermodynamic stability and its behaviour in solution remains uncertain and the effects have to be evaluated case by case.

In the present work, myoglobin of equine skeletal muscle, a single chain protein containing 153 amino acid residues, was selected for the synthesis of myoglobin-poly(ethylene glycol) conjugates. Such systems were studied by using differential scanning calorimetry and UV-visible spectroscopy in order to discriminate the thermodynamic contributions due to PEGylation on the overall protein stability, also focusing on the PEG's role on the solvent-protein surface interaction that dictate denaturation reversibility and/or aggregation phenomena. Despite the simple primary and tertiary structure (with 19 lysinic residues available for bioconjugation), this protein shows low thermal reversibility [25] and high tendency to aggregate after the thermal denaturation and represents a sensitive model with respect to the properties that we propose to investigate.

#### 2. Experimental section

#### 2.1. Materials

Myoglobin of equine skeletal muscle was purchased from Sigma Aldrich, whereas Dulbecco's phosphate buffered saline without calcium and magnesium (DPBS) was purchased from Gibco/Life Technologies (Germany) and used as received. Borate buffer 50 mM was prepared making a solution of sodium tetraborate 50 mM (distilled water and Na<sub>2</sub>B<sub>4</sub>O<sub>7</sub>·10H<sub>2</sub>O, Sigma Aldrich Germany); the pH was adjusted with HCl 0.1 M to pH = 8.8. Poly(ethylene glycol) monomethyl ether (PEG) ( $M_n$ = 5 kDa) was purchased from Fluka and post-modified following the procedure reported by Zalipski [26], obtaining N-hydroxysuccinimide-poly(ethylene glycol) (PEG-NHS). Sephadex G-50 medium (Sigma Aldrich) was allowed to soak in water overnight before use, following the proportion Sephadex/water= 10mL/50mL; when the column was not in use, it was stored in a solution of 5% EtOH at 4°C.

The synthesis and characterization of the PEGylated samples My-PEG (1) and My-PEG (2) was performed following a procedure reported in detail in the literature for analogue conjugates [27]. Suffice here to say that for the two bioconjugates we obtained purity = 99 %, dispersity D = 1.051, number-average molar mass  $M_n = 47.490$  and average number of attached chains = 3.3 for *My-PEG* (1), and purity = 97.5 %, dispersity D = 1.008, number-average molar mass  $M_n = 63.970$  and average number of attached chains = 5.2 for *My-PEG* (2).

#### 2.2. Differential Scanning Calorimetry (DSC)

Calorimetric measurements were carried out in solution with a protein concentration of about 1.5.10<sup>-4</sup> M in DPBS at pH 7.0 with a Setaram Micro-DSCIII apparatus, equipped with 1 mL hermetically closed cylindrical pans, at 0.5°C·min<sup>-1</sup> scan rate in the temperature range from 20°C to 95°C. Some measurements were also performed by using the TA Instruments Nano-DSC (6300) equipped with capillary cells at the same scan rate. For all experiments, a heating-cooling cycle was scheduled followed by a second heating scan. Data were analyzed by means of the software THESEUS [28] following procedures reported in previous studies [29]. Briefly, the apparent molar heat capacity  $C_P(T)$  of the sample was scaled taking as baseline the linear regression of the experimental data in the pre-denaturation region. The baseline subtraction provided the excess (with respect the native state) molar heat capacity  $C_P^{exc}(T)$  across the scanned temperature range. The heat capacity drop,  $\Delta_d C_P$ , across the signal was affected by a rather large error and was therefore not taken into account in the present work. The area underlying the recorded peaks, so treated, directly corresponds to the relevant denaturation enthalpy,  $\Delta_d H^\circ$ , in kJ·mol<sup>-1</sup> units. Errors were evaluated on the basis of at least three replicates. The fit attempts based on the denaturation thermodynamic models were accomplished using the nonlinear Levenberg–Marquardt method [30]. The errors of each fitting parameter were calculated with a 95.4% confidence limit by the Monte Carlo simulation method.

### 2.3. UV-Vis measurements

The UV-Vis absorbance spectra of the samples' solutions in DPBS were registered with a Jasco V-550 UV/VIS spectrometer in the range 200-600 nm. The initial protein concentration in the samples was between 1 and 1.5 mg/ml. The spectra were therefore normalized to the same protein concentration (1 mg/mL), using the intensity value recorded at 280 nm.

### 3. Results and discussion

3.1. Influence of bioconjugation on the reversibility of the protein thermal denaturation





Thermograms for unmodified myoglobin (1.5 ·10<sup>-4</sup>M in DPBS, pH 7.0, 0.5°C·min<sup>-1</sup> scan rate) obtained by using both a micro-DSC with cylindrical cell (blue curve) and a nano-DSC with capillary cells (red curve). The blue curve was smoothed in order to reduce the noise due to aggregation effects.

The blue curve in Fig. 1 reports the micro-DSC thermogram (with cylindrical cells) of the unmodified myoglobin. We observed a complex signal, namely an endothermic peak followed by a strong exothermic contribute ending with a noisy trace. This is a typical picture of overlapping processes, *i.e.* thermal denaturation of the protein with concomitant aggregation effect as expected for the myoglobin at this pH in line with the literature [31].

For sake of clarity and in an attempt to obtain information of the thermal stability of the protein in these conditions, despite the aggregation phenomena we also used a capillary cell DSC calorimeter and the resulting trace is reported in the same figure (red curve) showing a single endothermic peak. Indeed, the use of capillary cells seemed to mitigate the aggregation and/or precipitation phenomena. However, in both cases, the denaturation process was irreversible as revealed by the second heating scan (flat traces not reported).

These results were in agreement with the information obtained by the spectroscopic analysis (UV absorbance, 280 nm; extinction coefficient: 1.66 mg·cm<sup>-1</sup>, [32]). Indeed, the occurrence of a thermalinduced aggregation of myoglobin was confirmed by the determination of the protein concentration in solution before and after the thermal scan, which showed a consistent decrease in protein concentration after the calorimetric run (reduction of 45%) besides the formation of a visible red precipitate.





Micro-DSC thermograms for My-PEG (1) and My-PEG (2) solutions (1.5 ·10<sup>-4</sup>M in DPBS, pH 7.0, 0.5°C·min<sup>-1</sup> scan rate) in panel a and b, respectively. First heating scans from 20 to 95°C (blue curves); cooling scans from 95 to 20°C (purple curves); second heating scans from 20 to 95°C (red curves).

Fig. 2 reports the micro-DSC traces obtained through a heating/cooling cycle followed by a second heating scan for the My-PEG (1) and My-PEG (2) proteins (panel *a* and *b*, respectively). In both cases we observed a single endothermic peak corresponding to the protein thermal denaturation with no evident exothermic phenomena. However, the following cooling (purple curves) and the second heating (red curves) scans indicated only a partial reversibility of the process (smaller signals).

Nevertheless, despite the partial reversibility in these experimental conditions (heating up to 95°C), such a situation may correspond to a fully reversible process in the denaturation range, according to the literature [33]. In order to validate this hypothesis, a shorter heating/cooling cycle (up to 80°C) was performed for My-PEG (1) samples, followed by a complete second heating scan (Fig. 3). We observed that the first and the second heating scans were fully overlapped (blue and red curves, respectively) confirming that bioconjugation enhances the thermal denaturation reversibility of the protein. Moreover, the complete overlap between the second heating scan (red curve) and the first heating scan of the Fig.2a (reported in Fig. 3 as a grey trace) once again demonstrates our hypothesis and also verifies the reliability of the measurements. Again, these results were in agreement with the UV absorbance data. Indeed, the protein concentration in solution for the My-PEG (1) and My-PEG (2) samples was not significantly affected by the thermal scan.



#### Fig. 3: Assessment of the My-PEG denaturation reversibility.

Micro-DSC thermograms for My-PEG (1) solutions (1.5 ·10<sup>-4</sup>M in DPBS, pH 7.0, 0.5°C·min<sup>-1</sup> scan rate). First heating scan from 20 to 80°C (blue curve); second heating scan from 20 to 95°C (red curve). The first heating scan from 20 to 95°C (grey curve, which corresponds to the blue curve in Fig.2a) is also reported to highlight the reliability of the measurements.

Additional information on the bioconjugates in solution was provided by the UV-Vis absorption spectra of the samples in the wavelength range of 200-600 nm at room temperature. The absorbance spectra of My (black curve), My-PEG (1) (red curve) and My-PEG (2) (blue curve) are reported in Fig. 4 and indicate that the bioconjugation did not significantly affect the structure of the protein at room temperature. In particular, the profiles of all the samples presented a lower peak with the maximum at 280 nm and a more intense peak with the maximum at 409 nm. This second peak, called Soret band [34], is due to the absorbance of heme group and is exquisitely sensitive to changes in local environment [35]. The comparison between the spectra of myoglobin, My-PEG (1) and My-

PEG (2) recorded at room temperature showed only slight differences in the Soret band intensity. These slight differences, that reflects a local effect on the heme group, were the same in the two conjugates and seemed not to compromise the functionality of the protein at room temperature according to previous results of activity assays that showed a high preservation of the protein activity [27].



Fig. 4: Proteins spectroscopic characterization.

UV-Vis absorption spectra of the samples My (black curve), My-PEG (1) (red curve) and My-PEG (2) (blue curve), normalized per protein concentration.

#### 3.2. Thermodynamic analysis

The overall picture of My, My-PEG (1) and My-PEG (2) thermal unfolding is reported in Fig.5.





Thermograms from the first heating scan for My (capillary cells calorimeter), My-PEG (1), My-PEG (2) (circles curves from the right to the left, respectively) (1.5 ·10<sup>-4</sup>M in DPBS, pH 7.0, 0.5°C·min<sup>-1</sup> scan rate). The blue, green and red traces are the respective theoretical curves calculated according to a single step denaturation model.

It is evident that bioconjugation has a destabilizing effect on this protein as regards both the denaturation enthalpy and temperature that are significantly decreased (see Table 1).

The reversibility results of the PEGylated conjugates clearly indicate that a thermodynamic analysis of the denaturation mechanism is allowed [33]. Accordingly, thermodynamic models [36,37] were applied in order to describe the thermal denaturation of the PEGylated conjugates. A single step model native-to-denatured state was sufficient to obtain a good fit for the two protein-polymer conjugates. A tentative fit was also attempted on the unmodified myoglobin's trace obtained by the capillary calorimeter. No thermodynamic model produced a satisfactory fit confirming that, in this case, the capillary cell was not totally able to avoid aggregation phenomena. However, although the denaturation and the aggregation processes may be concomitant, we may assume that the beginning of the peak is not strongly affected by the exothermic contribute. Therefore, for the sake of completeness and being aware of the possible miscalculation in the case of the unmodified protein, an attempt of a single step fit of the early part of the thermogram is also reported in Fig. 5, according to the one-state denaturation fitting model. The best fit parameters obtained by these fitting attempts are also reported in Table 1.

System	Experimental		One state denaturation model Best-Fit parameters	
	$\Delta_d H^{\bullet} / kJ \cdot mol^{-1}$	$T_d / ^{\circ}\mathrm{C}$	$\Delta_d H^{\bullet} / kJ \cdot mol^{-1}$	$T_d / ^{\circ}\mathrm{C}$
Myoglobin	-	-	540	80.7
My–PEG (1)	$480 \pm 25$	$76.7\pm0.5$	485	76.7
<i>My</i> – <i>PEG</i> (2)	$415\pm25$	$73.1\pm0.5$	410	73.1

**Table 1:** Denaturation enthalpy,  $\Delta_d H^\circ$ , and temperature,  $T_d$ , obtained by experimental DSC traces and bestfit values for My, My-PEG (1) and My-PEG (2) samples. The fit parameters were calculated according to a one state denaturation model.

We may conclude that the destabilizing effect of the bioconjugation on this protein seems to follow the extent of the covalent modification, but do not alter the mechanism of thermal denaturation that remains a single step mechanism. Furthermore, taking into account the unaltered functionality of the proteins at room temperature [27], we may argue that the reduced thermodynamic stability of bioconjugated myoglobin, is mainly due to the altered solvent-surface interactions that mayaffect more the denatured state of the protein, that seems not to reach a complete random coil state because of the boundaries dictated by the bioconjugation, rather than to peculiar reorganizations of the native protein tertiary structure that remains functional at room temperature. This scenario is further supported by the reversibility enhancement in the case of both bioconjugate systems.

Formally, the protein functionality and thermodynamic stability is dictated by the  $\Delta_d G^{\circ}(T) = G_D^{\circ}(T) - G_N^{\circ}(T)$  equation [28], *i.e.* by the difference of the standard Gibbs energy between the denatured and the native state. Accordingly, the unaltered functionality of the proteins, at room temperature, suggests that this difference, *i.e.* the  $\Delta_d G^{\circ}(25^{\circ}C)$ , should remain the same for the three systems. Unfortunately, the DSC measurements of the proteins investigated in our conditions (see the experimental section) did not permit to directly measure the heat capacity drop,  $\Delta_d C_P$ , for the three systems, which represents an index of the solvent-exposed surface differences upon the denaturation [38–40] and in turn permits the  $\Delta_d G^{\circ}(25^{\circ}C)$  direct evaluation [28].

However, the calorimetric data ( $\Delta_d H^\circ$ ,  $T_d$ ) reported in Table 1 allowed to attempt a thermodynamic visualization of this scenario in relative terms, *i.e.* assuming, as reference, an arbitrary value for the  $\Delta_d C_P$  of the unmodified protein in the range of those reported in the literature [38–40] in order to evaluate the corresponding  $\Delta_d G^\circ(T)$ . In this way, the  $\Delta_d C_P$ , values for the PEGylated systems were estimated, *i.e.* by tentatively imposing the same  $\Delta_d G^\circ(25^\circ C)$  obtained for the unmodified myoglobin for the two bioconjugates. The results of this attempt are shown in Fig. 6. Of course, the absolute  $\Delta_d C_P$  values estimated for My-PEG (1) and My-PEG (2) depend on the  $\Delta_d C_P$  value of the unmodified protein, here arbitrarily chosen, but in any case and in relative terms, this scenario predicts a severe reduction of  $\Delta_d C_P$  for the PEGylated systems that follows the bioconjugation extent (Table 2), in line with all the experimental evidences in this work.



Fig. 6: Estimation of the standard Gibbs energy trends.

Calculated  $\Delta_d G^{\circ}(T)$  for My (blue curve), My-PEG (1) (green curve) and My-PEG (2) (red curve) according to the data reported in Table 1 and Table 2. The denaturation temperatures of My, My-PEG (1) and My-PEG (2) are respectively indicated as  $T_{d,0}$ ,  $T_{d,1}$  and  $T_{d,2}$ .

*Table 2:* Heat capacity drops,  $\Delta_d C_P$ , and their relative reduction for My-PEG (1) and My-PEG (2) estimated by assuming the same  $\Delta_d G^{\circ}(25^{\circ}C)$  for all the systems and a nominal  $\Delta_d C_P$  for My as reference.

System	$\Delta_d C_p / \mathbf{kJ \cdot mol^{-1} \cdot K^{-1}}$	Relative reduction
Myoglobin	7.5 <sup>a</sup>	-
My-PEG(1)	5.4	~30%
My–PEG (2)	1.9	~75%

<sup>a</sup> reference value assumed according to the literature [38–40].

#### Conclusions

The overall results of this study indicate that the bioconjugation process provides a thermal destabilization of myoglobin. However, such a modification does not alter the denaturation mechanism, which remains as a one-step process, and does not substantially compromise the protein native structure or its functionality. Moreover, the use of poly(ethylene glycol) as stealth agent

confers an enhanced reversibility to the denaturation process. The thermodynamic interpretation of the data indicated that the bioconjugation influences the solvent-exposed protein surface difference between native and denatured state. This variation seemed to follow the extent of the bioconjugation and is coherent with the prevention of aggregation phenomena and the consequent observed reversibility.

The calorimetric approach provides relevant complementary information for the overall characterization of new classes of protein-polymer conjugates as a base for the rational design of new drugs and for a deeper understanding of the behaviour of the conjugates in solution.

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### **Figure captions**

### Fig. 1: Myoglobin thermal denaturation.

Thermograms for unmodified myoglobin  $(1.5 \cdot 10^{-4} \text{M in DPBS}, \text{pH } 7.0, 0.5^{\circ}\text{C}\cdot\text{min}^{-1} \text{ scan rate})$  obtained by using both a micro-DSC with cylindrical cell (blue curve) and a nano-DSC with capillary cells (red curve). The blue curve was smoothed in order to reduce the noise due to aggregation effects.

### Fig. 2: PEGylation effect on the bioconjugates thermal stability.

Micro-DSC thermograms for My-PEG (1) and My-PEG (2) solutions  $(1.5 \cdot 10^{-4} \text{M in DPBS}, \text{pH 7.0}, 0.5^{\circ}\text{C}\cdot\text{min}^{-1}$  scan rate) in panel a and b, respectively. First heating scans from 20 to 95°C (blue curves); cooling scans from 95 to 20°C (purple curves); second heating scans from 20 to 95°C (red curves).

### Fig. 3: Assessment of the My-PEG denaturation reversibility.

Micro-DSC thermograms for My-PEG (1) solutions  $(1.5 \cdot 10^{-4}$ M in DPBS, pH 7.0,  $0.5^{\circ}$ C·min<sup>-1</sup> scan rate). First heating scan from 20 to 80°C (blue curve); second heating scan from 20 to 95°C (red curve). The first heating scan from 20 to 95°C (grey curve, which corresponds to the blue curve in Fig.2a) is also reported to highlight the reliability of the measurements.

### Fig. 4: Proteins spectroscopic characterization.

UV-Vis absorption spectra of the samples My (black curve), My-PEG (1) (red curve) and My-PEG (2) (blue curve), normalized per protein concentration.

### Fig. 5: Thermodynamic modelling of the DSC profiles.

Thermograms from the first heating scan for My (capillary cells calorimeter), My-PEG (1), My-PEG (2) (circles curves from the right to the left, respectively)  $(1.5 \cdot 10^{-4}$ M in DPBS, pH 7.0,  $0.5^{\circ}$ C·min<sup>-1</sup> scan rate). The blue, green and red traces are the respective theoretical curves calculated according to a single step denaturation model.

### Fig. 6: Estimation of the standard Gibbs energy trends.

Calculated  $\Delta_d G^{\circ}(T)$  for My (blue curve), My-PEG (1) (green curve) and My-PEG (2) (red curve) according to the data reported in Table 1 and Table 2. The denaturation temperatures of My, My-PEG (1) and My-PEG (2) are respectively indicated as  $T_{d,0}$ ,  $T_{d,1}$  and  $T_{d,2}$ .